

Multi-class Word Imagery Speech BCI Classification by Machine Learning, Operational Architectonics and Complex Networks

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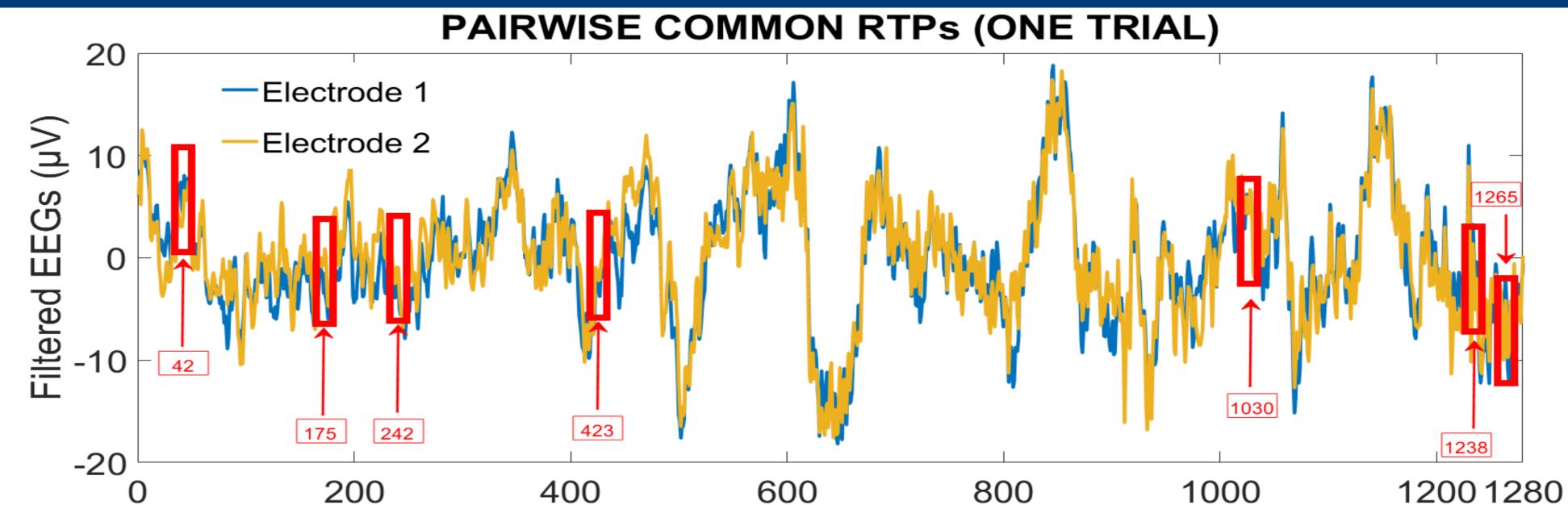


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1. INTRODUCTION

3. RESULTS

Speech imagery of electroencephalographic (EEG)based Brain Computer Interface (BCI) is significant for people with motor disabilities, illnesses and speech disorders. However, a reliable and efficient performance of these BCI systems depends strongly on the classification accuracy of speech imagery. Therefore, the development of more robust and consistent classification methods is



needed for improving communicating imagined		(0	20	0	400		600 Data Point	800 s (5 sec)	1000	120012
speech BCI systems.			•	•						electrodes for 23, 1030, 1238	
 2. METHODS Imagery pronunciation of 3 words ("<i>out</i>", "<i>in</i>", "<i>up</i>", 100 trials each, lasting for 5 sec) was performed by 5 	trial, w	here th		hts den			ed for on non RTP			2	
subjects [1]. EEG data sets (publicly available [1]) of 64 electrodes were recorded (10-20 system) and		C1	C2	C 3	C4		C60				
preprocessed (filtered and downsampled). The filtered EEG data of 60 channels (4 rejected	C1	0	7	4	4		5				
containing EOG artifacts) were analyzed based on a	C2	7	0	6	2		3				
novel classification algorithm comprised of "three pillars": a) Operational Architectonics (OA) concept of	C 3	4	6	0	5		6				
brain and mind functioning [2]. b) Complex network measures of brain connectivity [3]. c) Machine	C4	4	2	5	0		7				
Learning for developing multi-class classifiers. In										a of a waight	

particular, the off-line algorithm utilizes OA framework for a non-parametric segmentation of the filtered EEGs through the identification of abrupt jumps in EEG amplitude, called Rapid Transition (RTPs). Subsequently, the time Processes coordinates of RTPs are used to find the number of common RTPs in a trial with pairwise comparison of each filtered EEG. Then, these numbers are used as weights for the generation of weighted complex networks (60 x 60 adjacency matrix), from which 12 measures of brain connectivity are estimated for feature extraction. In the final step, these network metrics, properly normalized, form the feature vectors which are classified by a Naive Bayes classifier used for the prediction of each class. The results show that the overall mean classification

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Figure 2. An instance of a weighted complex network generated for one trial. The number on the edges denotes the weights of the adjacency matrix, while the number in the nodes indicate the channels.

Table 2 Five of the 12 Network Features estimated for 3 trials corresponding to different tasks, namely imagery pronunciation of "out", "in", "up".

	Mean Betweeness Centrality	Mean Clustering Coefficient	Mean Degree Centrality	Efficiency		Mean Strength
"out"	61.0333	4.9495	10.4333	5.09	•••	112.8667
" <i>in</i> "	80.6861	4.6908	8.5667	4.4490		92.1000
" <i>up</i> "	42.1278	5.3246	8.6667	3.6418		95.2667

Table 3 Overall mean classification accuracies (percentages) for all subjects estimated based on 10-fold cross validation procedure. The maximum accuracy is also shown in parentheses.

SUBJECTS	ACCURACY (%) (Chance Level = 33.33)
1	64.5 ± 7.6 (max = 83.33)

accuracies ranged approximately from 53.67% to	2	$53.67 \pm 7.7 (max = 66.67)$
66.17% (10-fold cross validation procedure),	\mathbf{O}	58.167 ± 7.68 (max = 73.33)
significantly above chance level (33.33%) in all		66.167 ± 9.2 (max = 80)
tested cases.	5	61.5 ± 7.37 (max = 76.67)

Selected References

[1] C H Nguyen, G K Karavas and P Artemiadis, Inferring imagined speech using EEG signals: a new approach using Riemannian manifold features. (2018) J. Neural Eng. 15:016002 (16pp). [2] A A Fingelkurts and A A Fingelkurts, Operational Architectonics Methodology for EEG Analysis: Theory and Results. (2015) Neuromethods 91: 1–59. [3] M Rubinov, O Sporns, Complex network measures of brain connectivity: Uses and interpretations. (2010) NeuroImage 52(3):1059-1069.

4. CONCLUSIONS

This study demonstrates a newly developed classification approach for decoding words during imagined speech production. Classifying imagined speech from EEG data is a difficult task, however, as shown, it is feasible to recognize features which distinguish words from information embedded in the EEG signals, with fairly good accuracies. More applications of the algorithm on new EEG-based BCI data sets are required to verify the aforementioned findings. Notwithstanding, the results are promising and may open a new perspective on the further development of EEG-based BCI systems for communicating imagined speech.